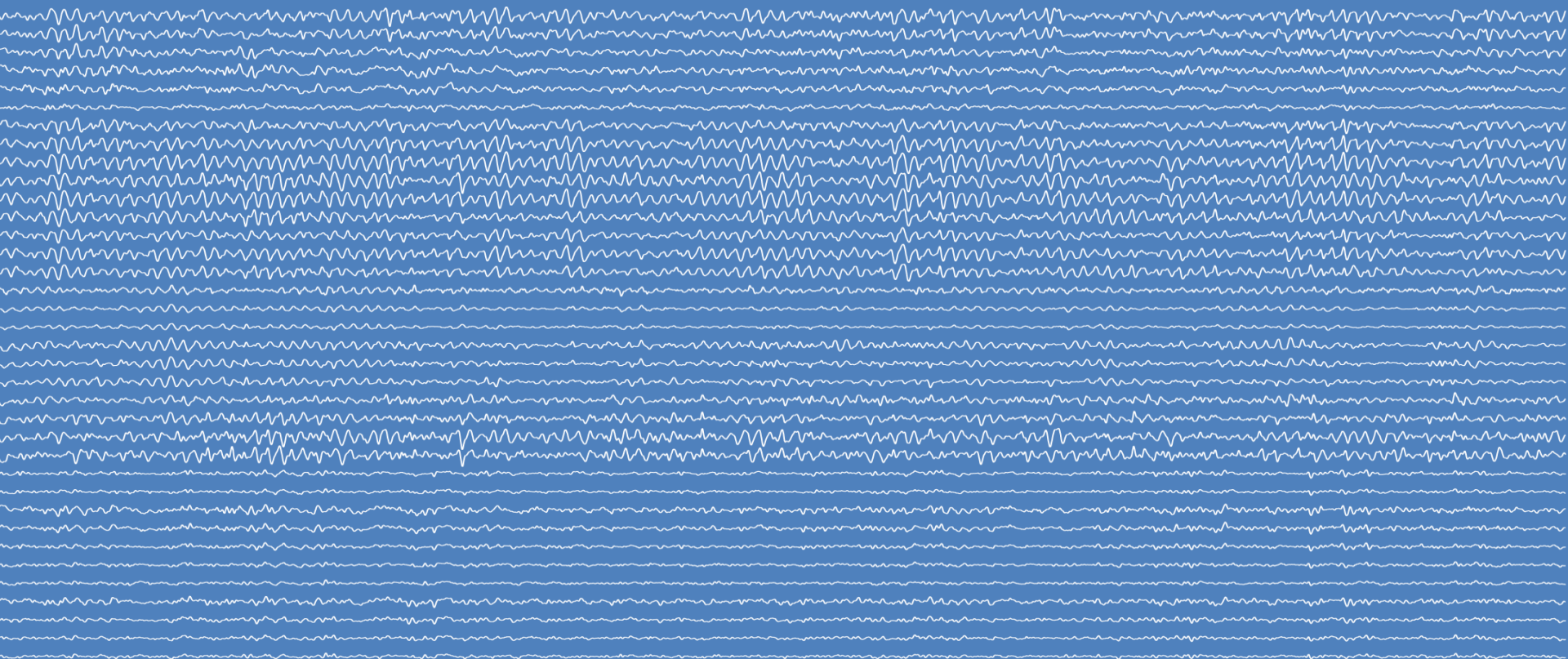


# Application of neural fields to EEG dynamics during general anesthesia

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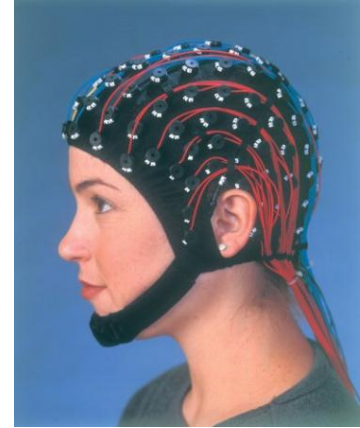
# Outline

- *Background on EEG*
- Neural field theory of the EEG
- EEG dynamics during general anesthesia

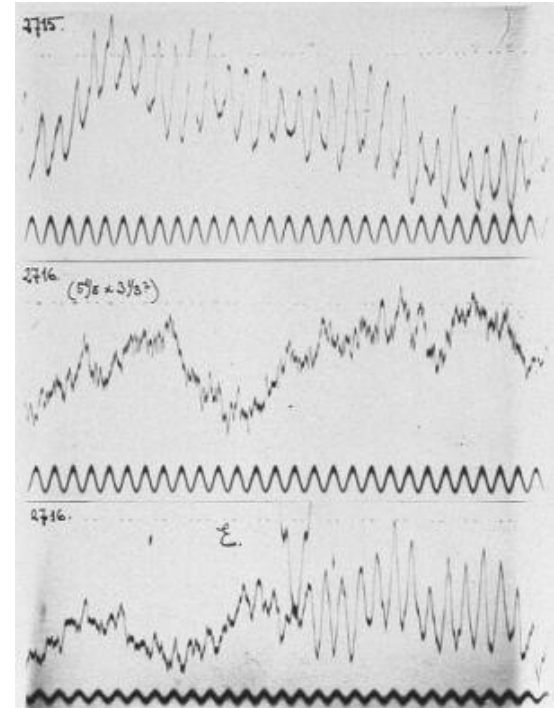
# EEG recordings

- *Electro-encephalography (EEG)* refers to electrical potentials recorded from the scalp
- First recorded in the 1920s by the German psychiatrist Hans Berger
- EEG reflects the total synaptic activity of large numbers of cortical pyramidal neurons

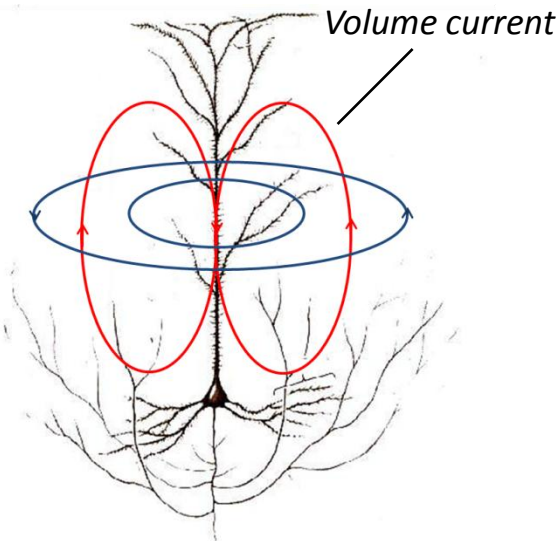
EEG electrode cap



First EEG recordings

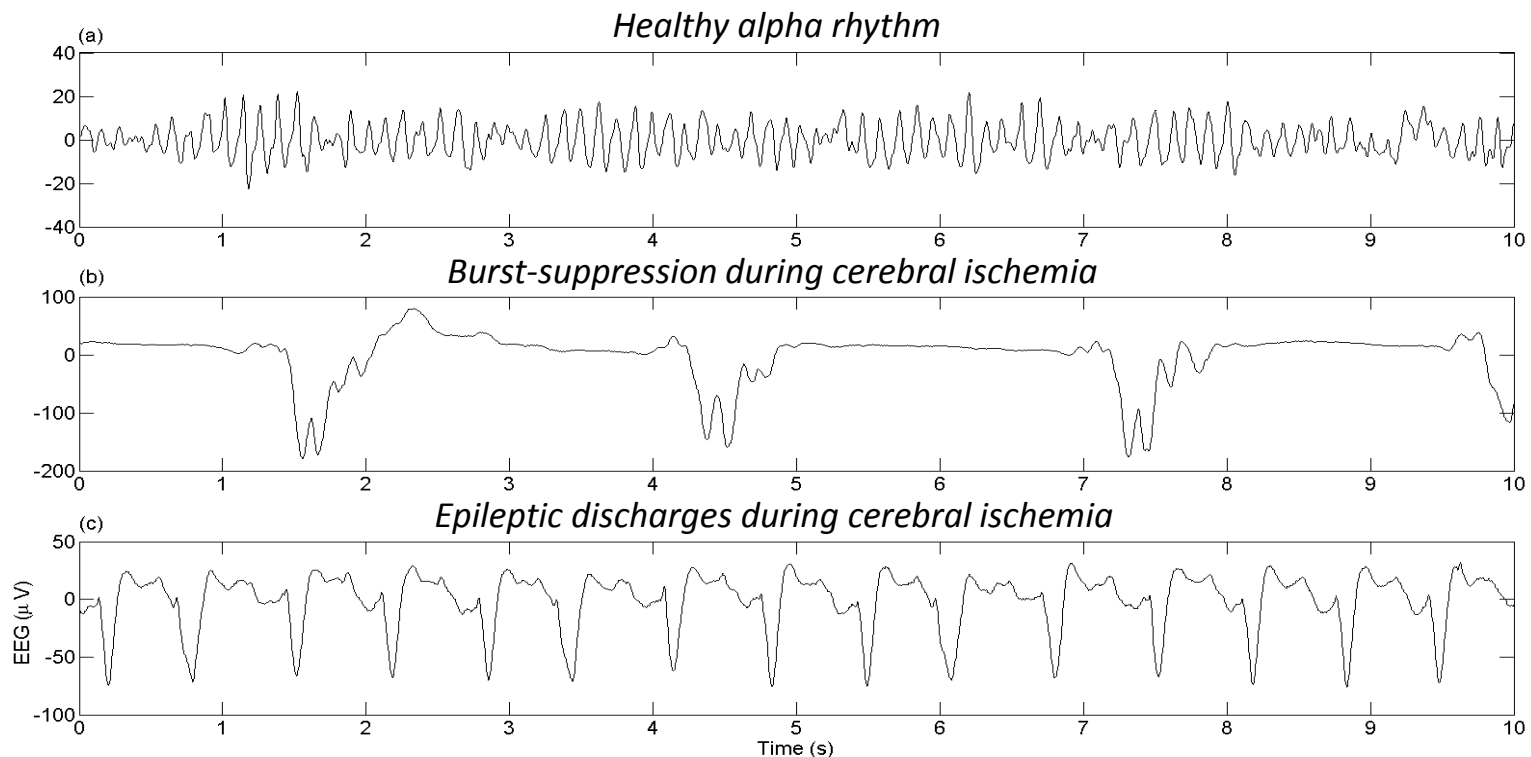


Hans Berger (1873-1941)



# Varieties of EEG rhythms

- There exist a wide variety of EEG rhythms
- Well documented correlations with cognitive and perceptual processes and neurological and psychiatric syndromes
- Functions and physiological mechanisms of generation remain poorly understood



# Outline

- Background on EEG
- *Neural field theory of the EEG*
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# Neural fields

- Neural fields describe the *macroscopic* spatio-temporal dynamics in cortical tissue
- State-variables are *mean membrane potential* (mV) and *mean firing-rate* (1/s) within cortical columns

- **Local dynamics:**

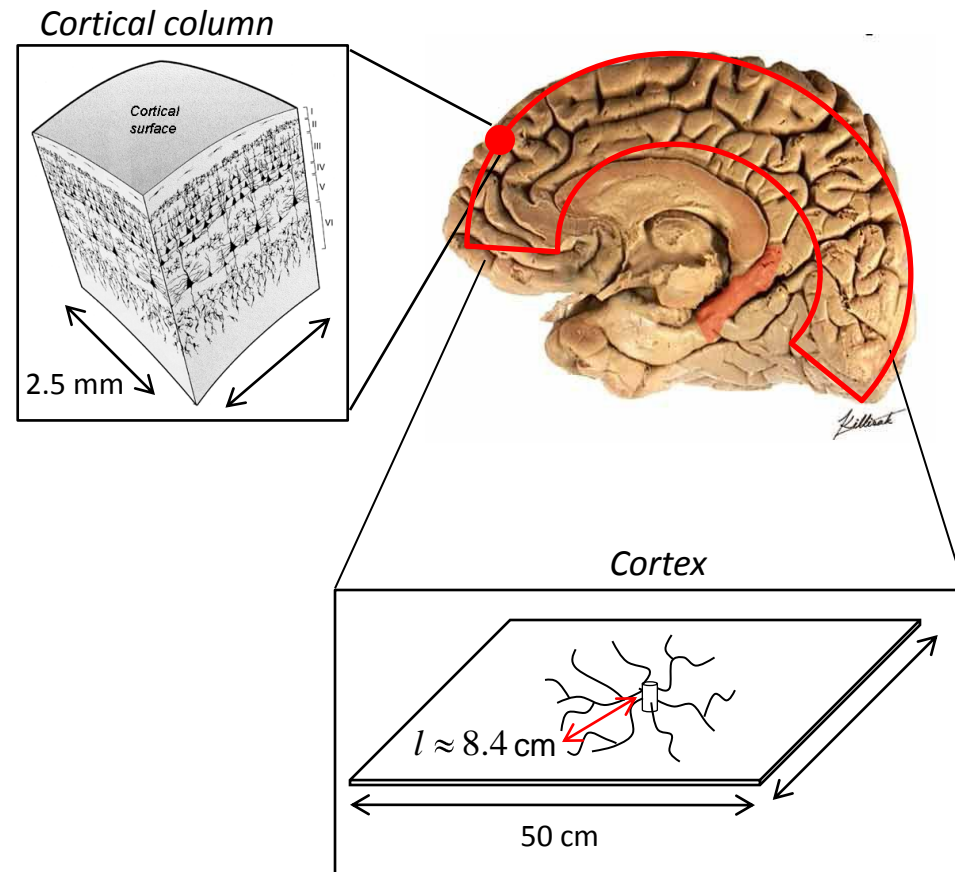
- synaptic filtering:  $V(t) = \nu h \otimes Q_{in}(t)$
- synaptic response:  $h(t) = \frac{\alpha\beta}{\beta - \alpha} [e^{-\alpha t} - e^{-\beta t}]$
- neural activation:  $Q(t) = S(V(t))$

- **Global dynamics:**

- Long-range cortico-cortical projections are modeled by

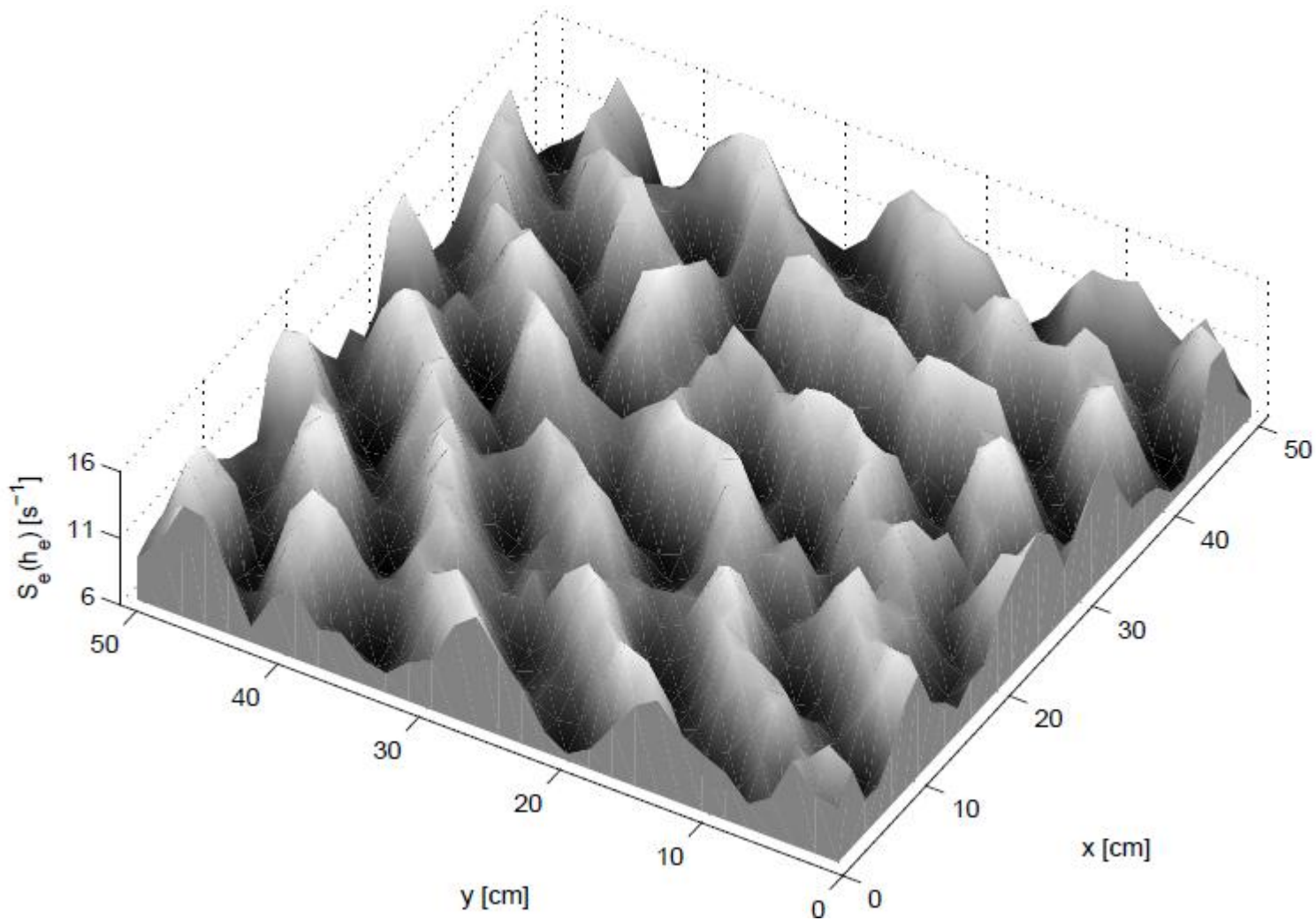
$$\phi(r, t) = \int_{-\infty}^t \int_{cortex} G(t, t', r, r') Q(t', r') dr' dt'$$

- Typically one assumes isotropy and constant conduction velocity:  $G(\|r - r'\|, t - \frac{\|r - r'\|}{v})$



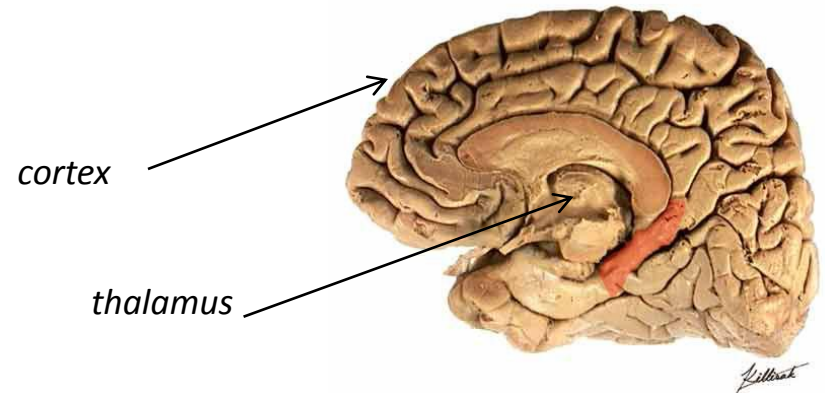


# Simulation of alpha rhythm

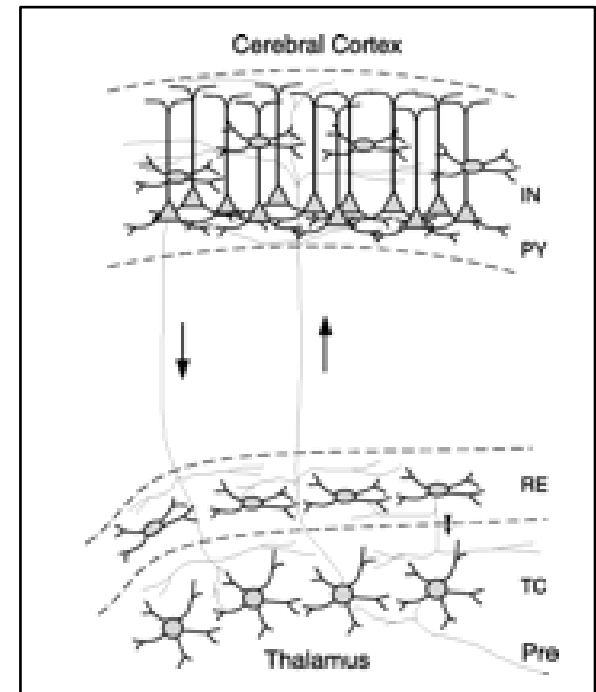


# Beyond cortical chauvinism

- Most field theories of large-scale brain dynamics (EEG) treat the cortex as an anatomically isolated structure (Liley, 2002)
- However, cortex is densely and reciprocally connected to the thalamus
- In (Robinson, 2001; Rennie, 2002) a new direction was initiated by developing a thalamo-cortical field theory of the EEG
- Besides spontaneous EEG rhythms, the model can reproduce sleep spindles, evoked responses, and generalized seizures (Robinson, 2001; Rennie, 2002)
- Propofol targets subcortical structures and imaging studies (PET and fMRI) suggest that the thalamus is involved in anesthesia-induced functional changes in cortex



*Thalamo-cortical connectivity*





# Thalamo-cortical field equations

$$V_e(x, t) = \bar{h} \otimes v_{ee} \phi_e(x, t) + \bar{h} \otimes v_{es} S(V_s(x, t - \tau/2)) + \bar{h} \otimes v_{ei} S(V_i(x, t)),$$

$$V_i(x, t) = \bar{h} \otimes v_{ie} \phi_e(x, t) + \bar{h} \otimes v_{is} S(V_s(x, t - \tau/2)) + \bar{h} \otimes v_{ii} S(V_i(x, t)),$$

$$V_s(x, t) = \bar{h} \otimes v_{sn} \phi_n(x, t) + \bar{h} \otimes v_{se} \phi_e(x, t - \tau/2) + \bar{h} \otimes v_{sr} S(V_r(x, t)),$$

$$V_r(x, t) = \bar{h} \otimes v_{rs} S(V_s(x, t)) + \bar{h} \otimes v_{re} \phi_e(x, t - \tau/2),$$

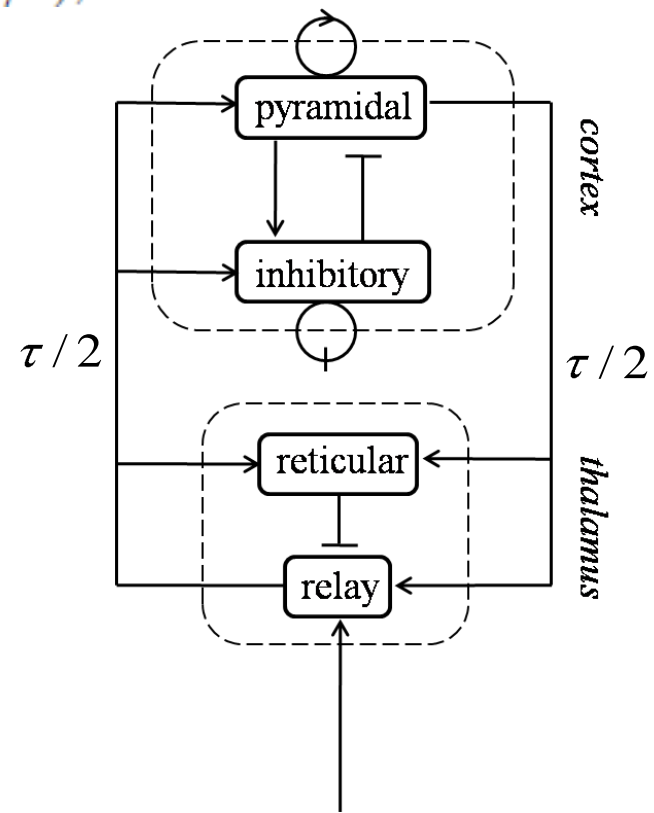
$$D(x, t) \phi_e = S(V_e),$$

where  $D$  is the wave operator

$$D = \left( \frac{1}{\gamma} \frac{\partial}{\partial t} + 1 \right)^2 - l^2 \nabla^2$$

with  $\gamma = v/l$  the cortical damping rate (1/s)

- Approximately, the EEG signal is proportional to  $\phi_e$



# Linearization and EEG spectra

- The transfer function from  $\phi_n$  to  $\phi_e$  is given by

$$\frac{\phi_e}{\phi_n} = \frac{\zeta_{eism} + (1 - \zeta_{ii})\zeta_{esn}}{[(D - \zeta_{ee})(1 - \zeta_{srs}) - \zeta_{ese} - \zeta_{esre}](1 - \zeta_{ii}) - \zeta_{eie}(1 - \zeta_{srs}) - \zeta_{eise} - \zeta_{eisre}}$$

↖  
Laplace transform  
of wave operator  
( $k = (0,0)$ )

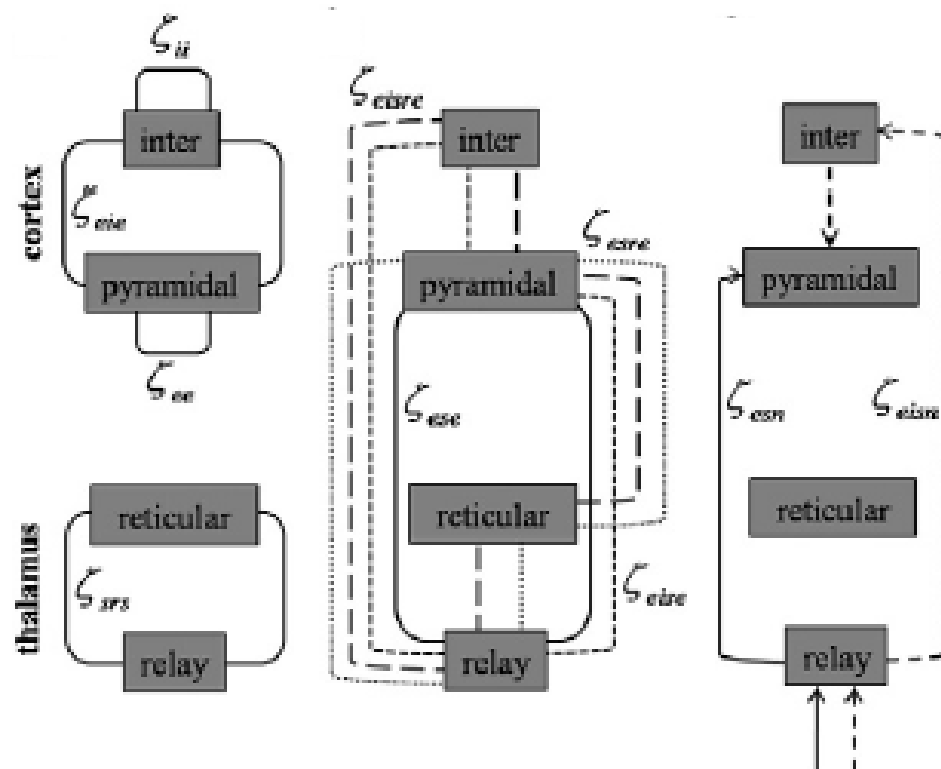
↖  
frequency response  
in the anatomical  
loop  $e \rightarrow s \rightarrow e$

- For  $\phi_n$  white noise:

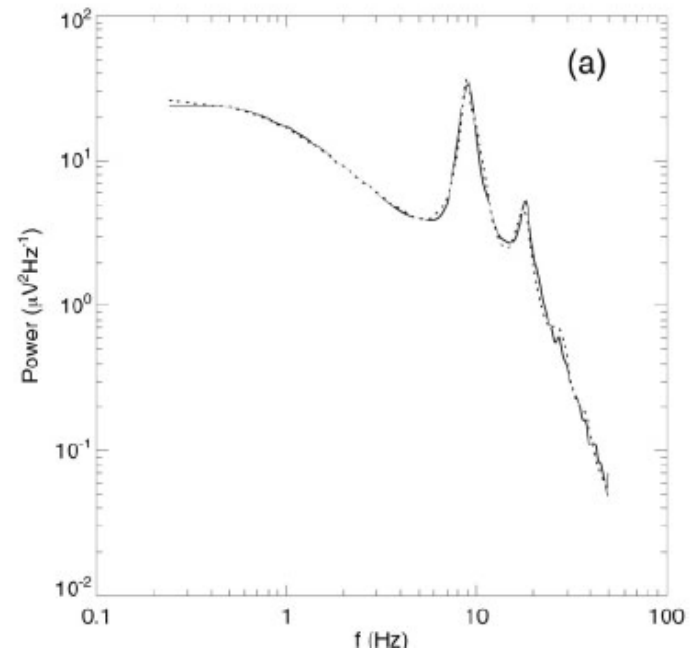
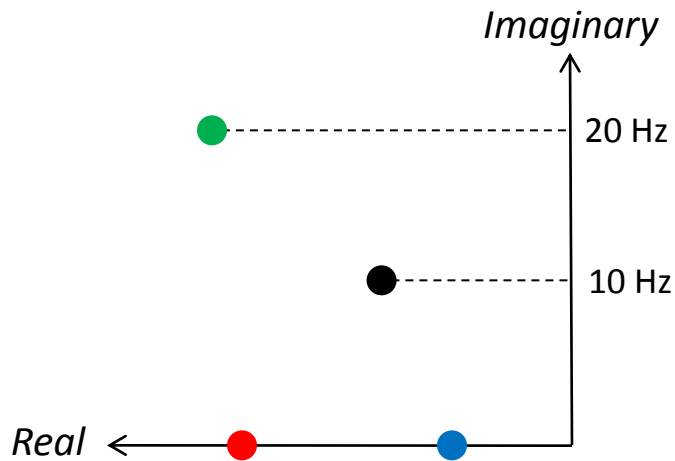
$$\phi_n = \langle \phi_n \rangle + \sigma_n \xi(t)$$

the EEG power spectrum is given by

$$P(\omega) = \sigma_n^2 |\phi_e(\omega)|^2$$



# Resonances underlying EEG spectra



(Robinson, P. et al., Human Brain Mapping 2004)

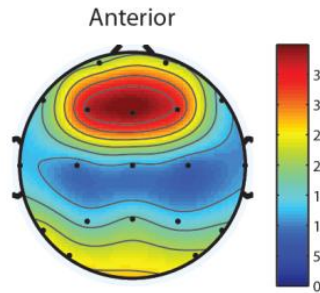
The EEG power spectrum during wakefulness is dominated by the following resonances:

- ● - **a pair of non-oscillatory resonances** (underlying the power-law decay of EEG spectra)
- - **alpha resonance** (underlying the spontaneous alpha rhythm)
- - **beta resonance** (underlying the first harmonic of the alpha rhythm)

# Outline

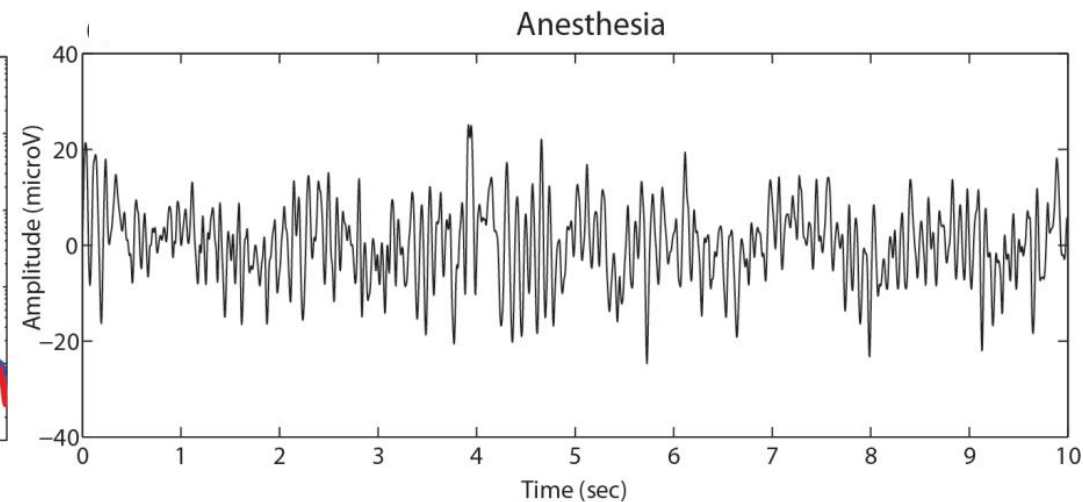
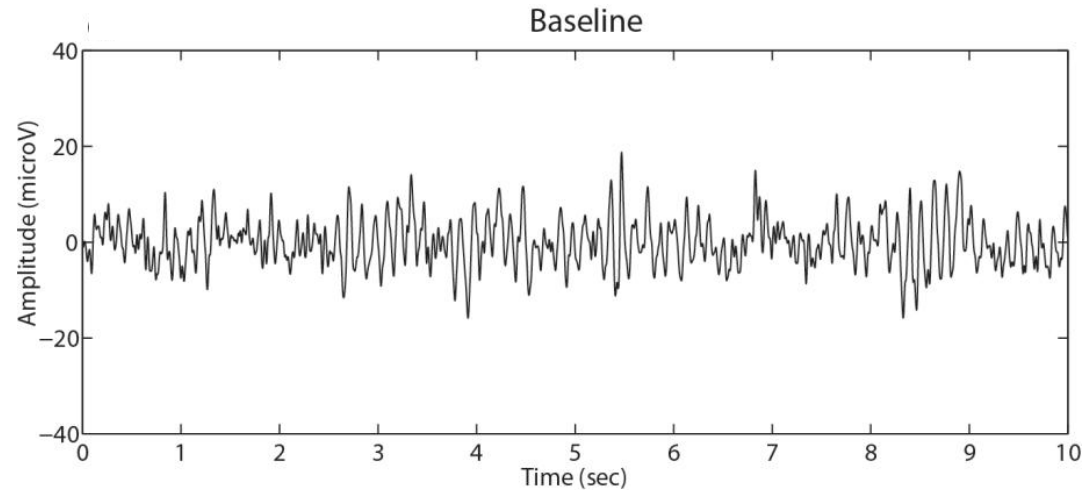
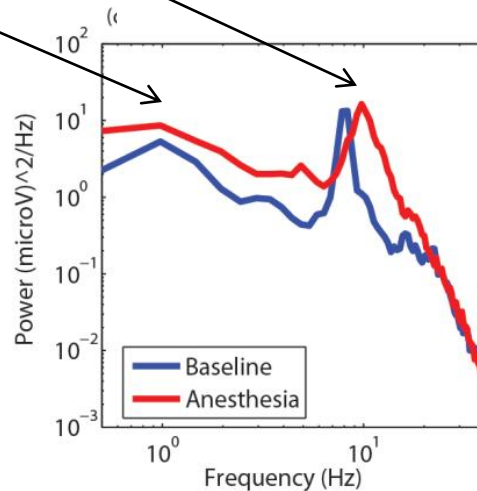
- Background on EEG
- Neural field theory of the EEG
- *EEG dynamics during general anesthesia*

# EEG phenomenology

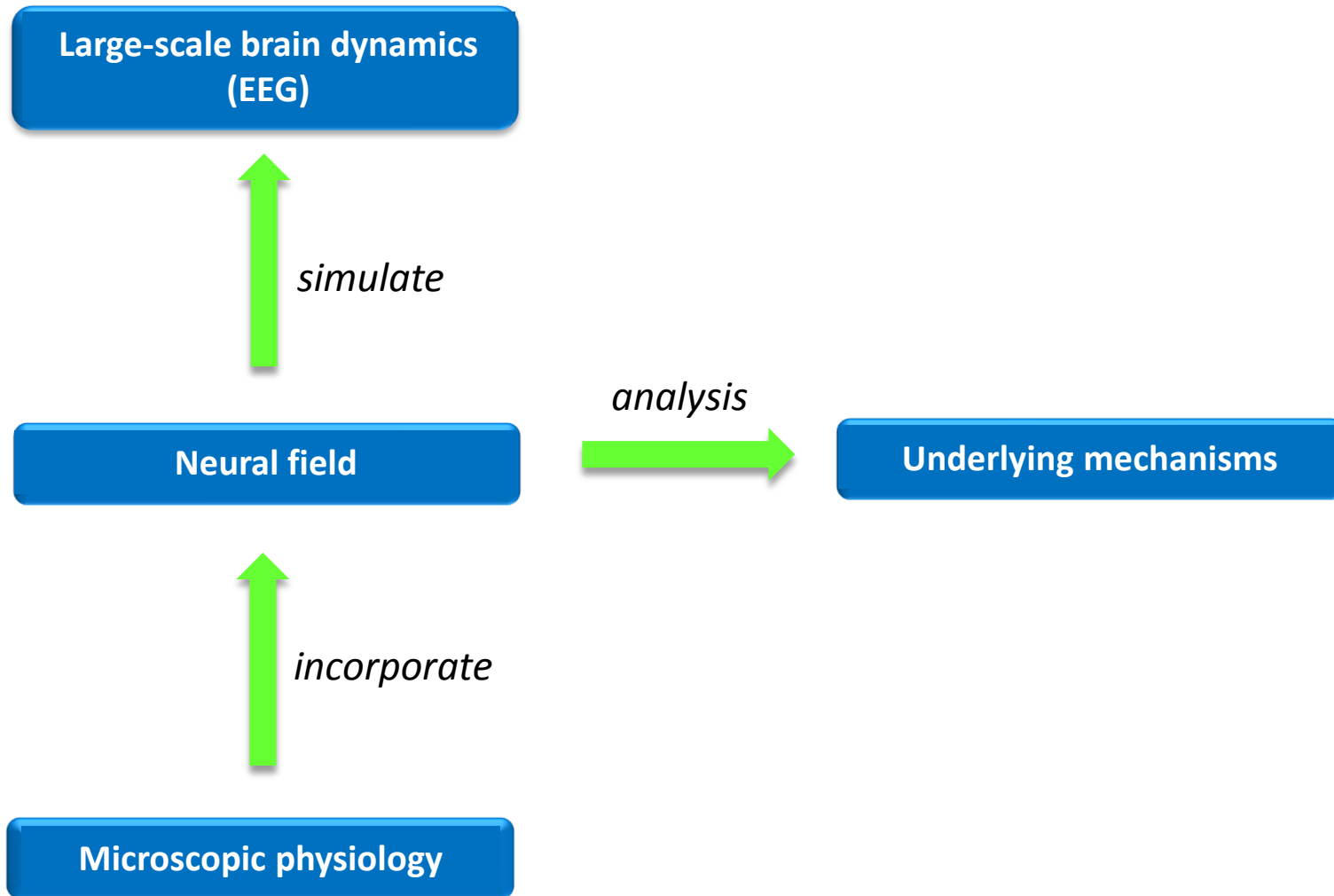


Pronounced frontal alpha oscillations (7 – 13 Hz) with increased peak-frequency

Increased delta (0.5 – 3 Hz) and theta (3 – 7 Hz) power



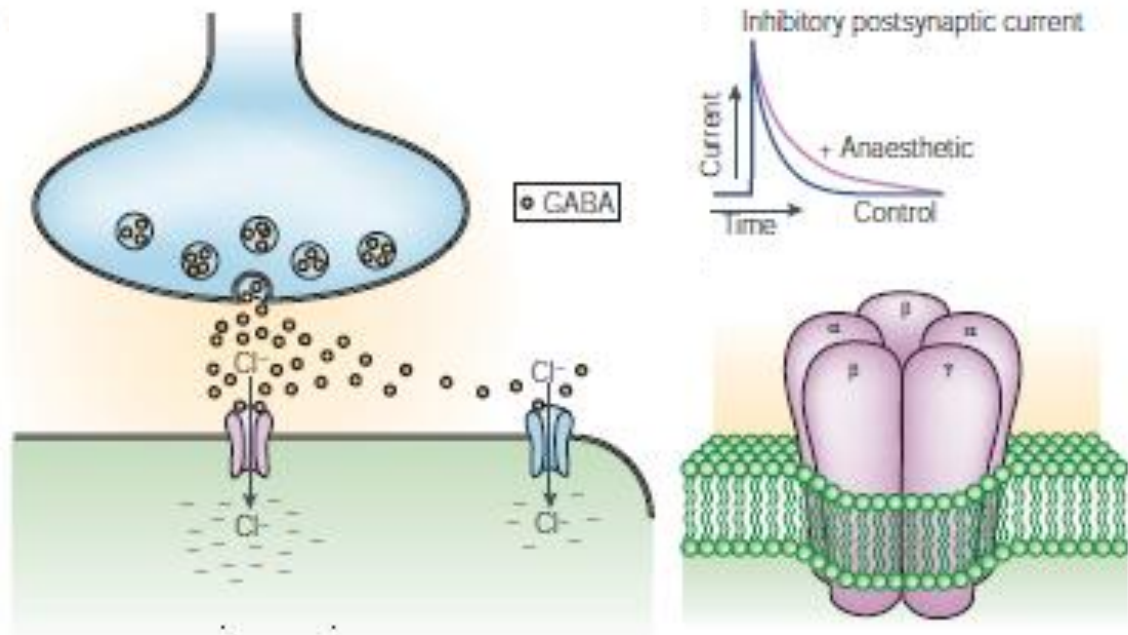
# Crossing scales



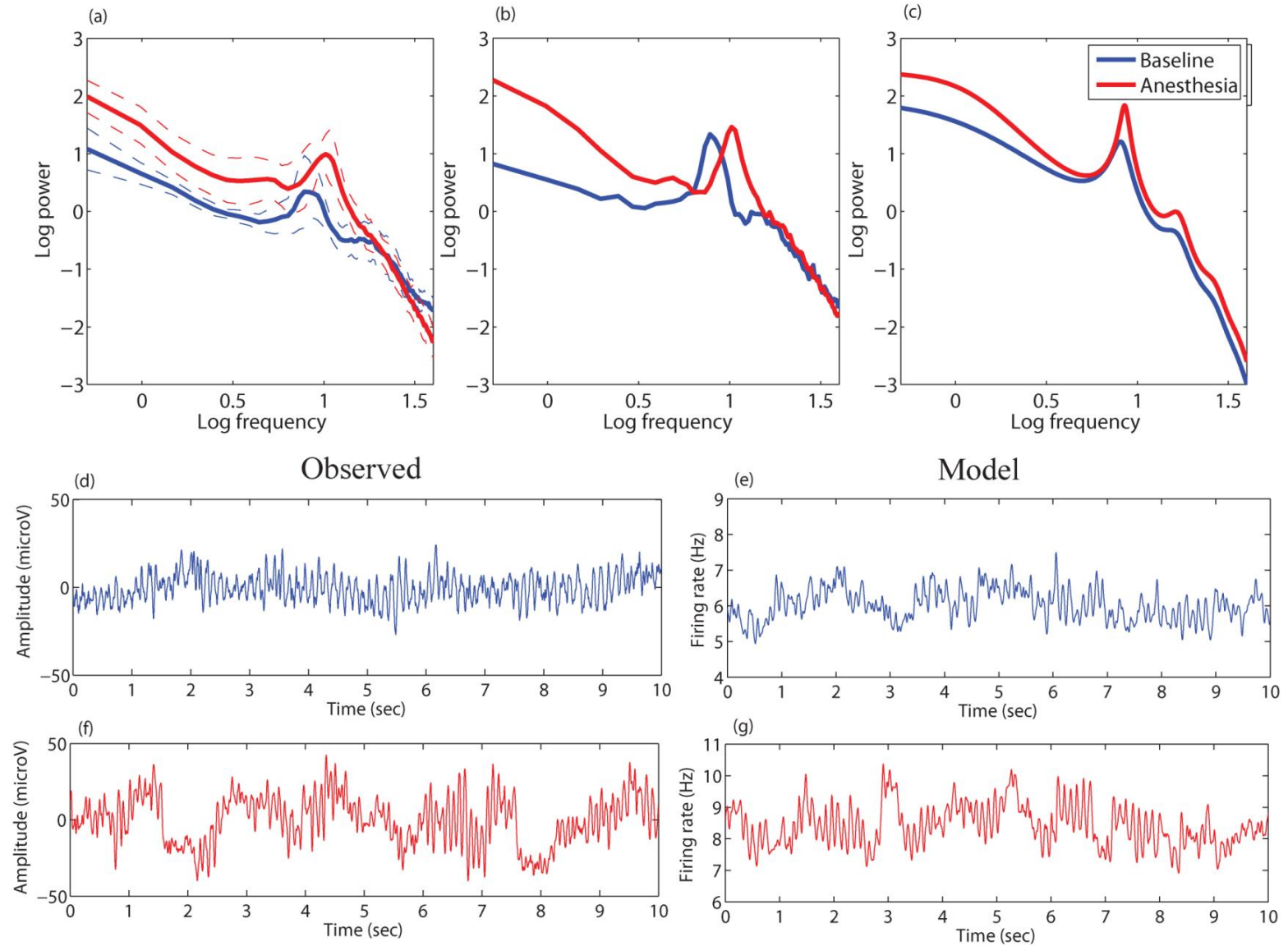


# The action of propofol

- Propofol pre-dominantly targets GABA<sub>A</sub> receptors
- It increases the time-constant of receptor de-activation
- About a dozen GABA<sub>A</sub> receptor subtypes
- Differential affinity is not completely known

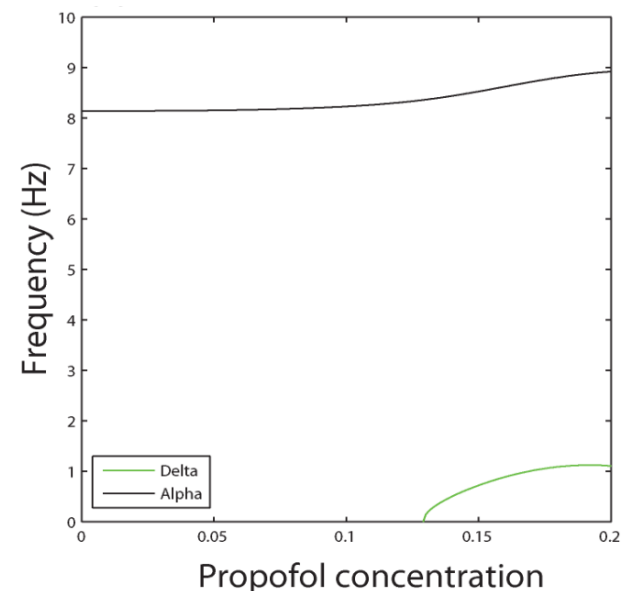
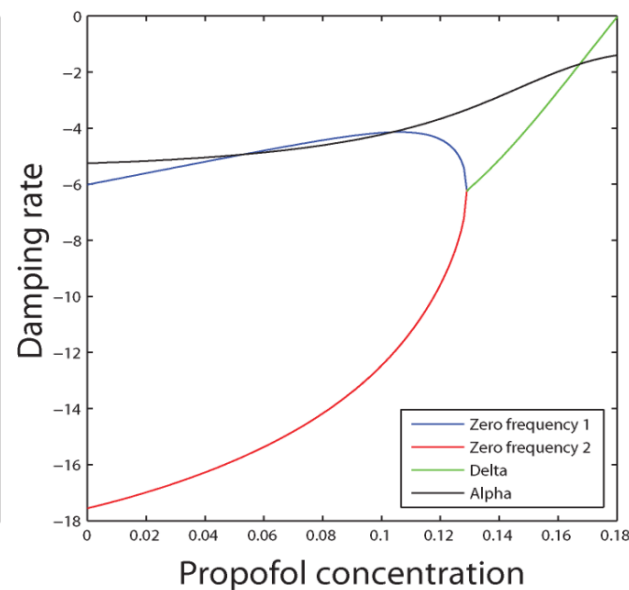
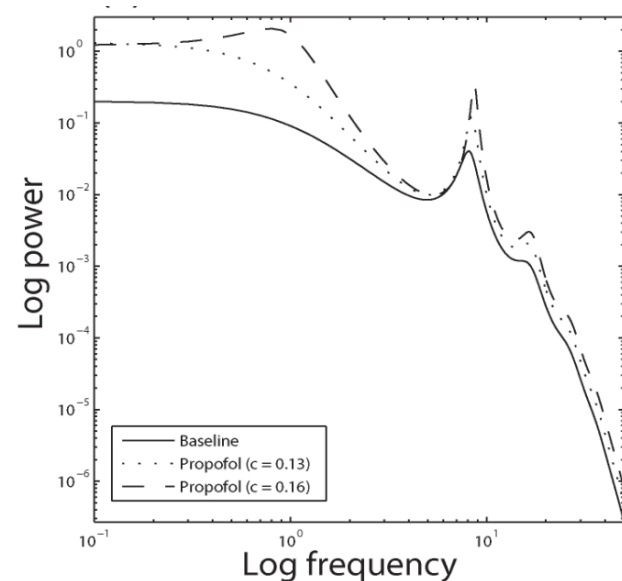


# Reproduction of experimental observations

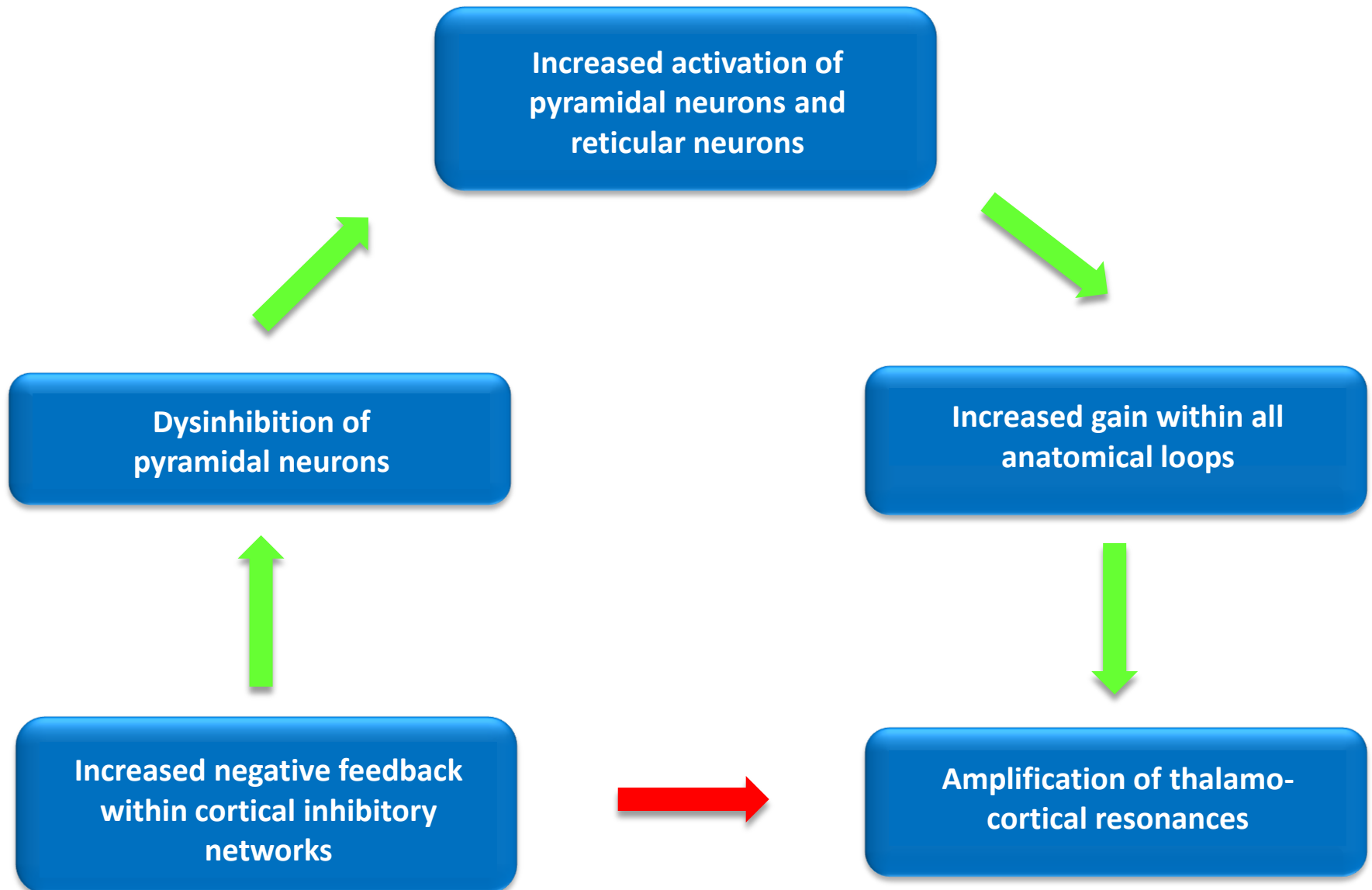


# Modulation of resonances

- Pronounced EEG alpha (7-13 Hz) oscillations are caused by amplification of the alpha resonance
- Increased EEG delta power (0.5-3 Hz) is caused by the net amplification of the pair of non-oscillatory resonances
- Increased EEG theta power (3-7 Hz) is caused by spectral leakage



# Underlying mechanisms



# Model predictions

- *Propofol has a higher affinity for receptors on interneurons than for receptors on pyramidal neurons*
- *Selective administration of propofol to cortical tissue leads to the observed EEG phenomenology*
- *Increased firing-rates of pyramidal neurons in frontal cortex and neurons within reticular nuclei*
- *Increased synchrony of alpha oscillations between frontal cortex and thalamic nuclei*

