# BUGS/WBDiff software: Bayesian inference for dynamical systems

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#### Outline

- The BUGS project
  - mathematical framework graphical models/Gibbs sampling
  - underlying philosophy
- WinBUGS Differential Interface (WBDiff)
  - illustration with pharmacokinetic models
- Applied examples
  - insulin/glucose/acipimox data
  - interstitial-/plasma-glucose data
  - experimental epidemiology host-parasite system
- Conclusions + future work...

#### Graphical models: linear regression example



 $y_i \sim \mathsf{N}(\mu_i, \tau^{-1}) \qquad \mu_i = \alpha + \beta x_i \qquad i = 1, ..., \mathsf{N}$  $\alpha \sim p(\alpha) \qquad \beta \sim p(\beta) \qquad \tau \sim p(\tau)$  $\operatorname{eg} \mathsf{N}(0, 100^2) \qquad \operatorname{eg} \mathsf{N}(0, 100^2) \qquad \operatorname{eg} \mathsf{Ga}(\epsilon, \epsilon)$ 

#### Why?

- Can describe (pictorially) very wide class of models with Directed Acyclic Graphs (DAGs) – links are directed and there are no cycles
- Obvious benefit when models become complicated
- Convey essential structure of problem without recourse to large set of equations
- Achieved through abstraction hiding of detail
- Graph encodes series of conditional independence assumptions

 $v \perp$  non-descendants[v]|parents[v]

which allow properties of model to be derived abstractly – more later...

#### Linear regression example

► Bayes' Theorem:

$$p(\theta|y) \propto p(\theta)p(y|\theta)$$

$$p(\alpha, \beta, \tau|y) \propto p(\alpha)p(\beta)p(\tau)\prod_{i=1}^{N} N(\alpha + \beta x_i, \tau^{-1})$$

Full conditional distributions (for Gibbs sampling):

$$p(\alpha|\beta,\tau,y) \propto p(\alpha) \prod_{i=1}^{N} N(\alpha + \beta x_i, \tau^{-1})$$
$$p(\beta|\alpha,\tau,y) \propto p(\beta) \prod_{i=1}^{N} N(\alpha + \beta x_i, \tau^{-1})$$
$$p(\tau|\alpha,\beta,y) \propto p(\tau) \prod_{i=1}^{N} N(\alpha + \beta x_i, \tau^{-1})$$

#### More generally...

► For any DAG:

 $p(V) = \prod_{v \in V} p(v | parents[v])$  [factorization theorem]

where V is the set of all nodes

• Note that  $p(\theta|y) \propto p(\theta, y) = p(V)$ 

• Also 
$$FCD(w) = p(w|V \setminus w) \propto p(V)$$

 $\Rightarrow \mathsf{FCD}(w) \propto p(w|\mathsf{parents}[w]) \times \prod_{v \in \mathsf{children}[w]} p(v|\mathsf{parents}[v])$ 

#### Factorization theorem

- Beauty of FT is two-fold:
  - (i) can write down joint posterior for any DAG simply by knowing relationship between each node and its parents
  - (ii) full conditional is *local computation* on the graph, involving only the node-parent dependencies for node of interest and its children



#### Combining models

- Only need to consider small part of model at any given time; no need to take account of bigger picture...
- Can construct arbitrarily complex structures by combining submodels together – mechanism of inference remains the same



# BUGS

- ► BUGS: Bayesian inference Using Gibbs Sampling
- Provides language for specifying parent-child relationships
- Uses (inverts) these to calculate full conditional distributions

```
st(

N = 20,

prec = 0.0001,

a = 0.001, b = 0.001,

y = c(1.3, 2.4, ...),

x = c(9.7, 5.9, ...)
```

# Differential equation models: e.g. 'one-compartment' pharmacokinetic model



#### One-compartment model, solution

$$C_b(t) = rac{Dose}{V_b} imes rac{k_a}{k_e - k_a} \left\{ \exp(-k_a t) - \exp(-k_e t) \right\}$$



#### Physiologically based PK model



$$\begin{array}{lcl} \displaystyle \frac{dA_{LU}}{dt} & = & Q_{LU} \times (C_{VEN} - C_{LU}/Kp_{LU}) \\ \displaystyle \frac{dA_{hkb}}{dt} & = & Q_{hkb} \times (C_{ART} - C_{hkb}/Kp_{hkb}) - RE(t) \\ \displaystyle \frac{dA_{gsps}}{dt} & = & Q_{gsps} \times (C_{ART} - C_{gsps}/Kp_{gsps}) \\ \displaystyle \frac{dA_{LI}}{dt} & = & Q_{H} \cdot C_{ART} + Q_{gsps} \cdot C_{gsps}/Kp_{gsps} + RA(t) \\ & & - Q_{LI} \cdot C_{LI}/Kp_{LI} - RM(t) \\ \displaystyle \frac{dA_{AD}}{dt} & = & Q_{AD} \times (C_{ART} - C_{AD}/Kp_{AD}) \\ \displaystyle \frac{dA_{ART}}{dt} & = & Q_{LU} \cdot C_{LU}/Kp_{LU} - CO \cdot C_{ART} \\ \displaystyle \frac{dA_{VEN}}{dt} & = & Q_{hkb} \cdot C_{hkb}/Kp_{hkb} + Q_{LI} \cdot C_{LI}/Kp_{LI} \\ & + & Q_{mbst} \cdot C_{mbst}/Kp_{mbst} \\ \displaystyle + & Q_{AD} \cdot C_{AD}/Kp_{AD} + RI(t) - Q_{LU} \cdot C_{VEN} \end{array}$$

# BUGS language specification

$$\frac{dA_g}{dt} = -k_a A_g \qquad \frac{dA_b}{dt} = k_a A_g - k_e A_b \qquad [A_g(0) = Dose, A_b(0) = 0]$$
model {
for (i in 1:N) {
 y(i] ~ dnorm(Cb[i], tau)
 Cb[i] <- solution[i, 2] / Vb
}
solution[1:N, 1:2] <- ode(init[], grid[], D(A[1:2], t), origin, tol)
D(A[1], t) <- -ka \* A[1]
D(A[2], t) <- ka \* A[1] - ke \* A[2]
# solution[1:N, 1:2] <- one.comp(init[], grid[], theta[], origin, tol)
# theta[1] <- ka; theta[2] <- ke
init[1] <- dose; init[2] <- 0
ke ~ dunif(0, 10)
ka ~ dunif(0, 10)
Vb ~ dunif(0, 100)
sd ~ dunif(0, 10)
tau <- 1 / pow(sd, 2)
}

# BUGS language specification

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\frac{dA_g}{dt} = -k_a A_g \qquad \frac{dA_b}{dt} = k_a A_g - k_e A_b \qquad [A_g(0) = Dose, \quad A_b(0) = 0]
model {
  for (i in 1:N) {
    v[i] ~ dnorm(Cb[i], tau)
    Cb[i] <- solution[i, 2] / Vb
  }
# solution[1:N, 1:2] <- ode(init[], grid[], D(A[1:2], t), origin, tol)</pre>
# D(A[1], t) <- -ka * A[1]
   D(A[2], t) <- ka * A[1] - ke * A[2]
#
  solution[1:N, 1:2] <- one.comp(init[], grid[], theta[], origin, tol)
  theta[1] <- ka; theta[2] <- ke
  init[1] <- dose; init[2] <- 0
  ke ~ dunif(0, 10)
  ka ~ dunif(0, 10)
  Vb ~ dunif(0, 1000)
  sd \sim dunif(0, 10)
  tau <- 1 / pow(sd, 2)
}
```

#### Source code (template)

MODULE WBDiffOneComp;

IMPORT WBDiffODEMath, Math;

TYPE

Equations = POINTER TO RECORD (WBDiffODEMath.Equations) END; Factory = POINTER TO RECORD (WBDiffODEMath.Factory) END;

CONST

nEq = 2;

```
VAR
```

fact-: WBDiffODEMath.Factory;

PROCEDURE (e: Equations) Derivatives (IN theta, A: ARRAY OF REAL; n: INTEGER; t: REAL; OUT dAdt: ARRAY OF REAL);

```
VAR
ka, ke: REAL;
BEGIN
ka := theta[0]; ke := theta[1];
dAdt[0] := -ka * A[0];
dAdt[1] := ka * A[0] - ke * A[1];
END Derivatives;
```

.....

#### Source code continued

PROCEDURE (e: Equations) Derivatives (IN theta, A: ARRAY OF REAL; n: INTEGER; t: REAL; OUT dAdt: ARRAY OF REAL);

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```

#### Another example: insulin/glucose kinetics

- Insulin produced by pancreas to stimulate glucose transport into and utilisation by cells
- Intravenous glucose tolerance test (IVGTT) used to measure sensitivity of glucose disappearance to insulin
- Administer bolus dose of glucose and monitor blood-glucose and blood-insulin concentrations
- Fit minimal model...

#### Minimal model for glucose kinetics



#### Minimal model continued

- Reparameterize slightly...
- ▶ Define insulin sensitivity S<sub>1</sub> = p<sub>3</sub>/p<sub>2</sub> and glucose effectiveness S<sub>G</sub> = p<sub>1</sub>
- Also let  $Z = X/S_I$

$$\frac{dG}{dt} = -S_G(G(t) - G_b) - S_I Z(t) G(t) \quad \frac{dZ}{dt} = p_2 \{ (I(t) - I_b) - Z(t) \}$$

- S<sub>G</sub>: combined effect of glucose to enhance glucose uptake and suppress endogenous glucose production at basal insulin levels
- ► *S*<sub>1</sub>: insulin's action to accelerate glucose uptake and suppress glucose production

#### Implementation

- We have observed values of G and I at various times  $+ G_b$ ,  $I_b$  and  $G_0$
- Solve equations for G and Z
- ► I(t) is a forcing function, need to evaluate at arbitrary times → interpolate between observed values? Fit spline?
- Currently no way to define 'functions' in BUGS language (except for derivatives)
  - $\rightarrow$  have to 'hard-wire' equations...

#### Implementation

```
PROCEDURE Interpolate (IN time, insulin: ARRAY OF REAL; t: REAL;
OUT x: REAL);
```

END Interpolate;

PROCEDURE (e: Equations) Derivatives (IN theta, A: ARRAY OF REAL; n: INTEGER; t: REAL; OUT dAdt: ARRAY OF REAL);

```
VAR
```

```
time, insulin: ARRAY 22 OF REAL;

Gb, lb, SI, SG, p2, lt: REAL; i: INTEGER;

BEGIN

i:= 0;

WHILE i < 22 DO

time[i] := theta[i]; insulin[i] := theta[22 + i];

INC(i)

END;

Gb := theta[44]; lb := theta[45];

SI := theta[46]; SG := theta[47]; p2 := theta[48];

Interpolate(time, insulin, t, lt);

dAtt[0] := -SG*(A[0] - Gb) - SI*A[1]*A[0];

dAtt[1] := p2*((It - Ib) - A[1]);

END perivatives:
```

$$\frac{dG}{dt} = -S_G(G(t) - G_b) - S_I Z(t) G(t) \quad \frac{dZ}{dt} = p_2 \{ (I(t) - I_b) - Z(t) \}$$

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#### BUGS code

```
model {
 for (i in 7:N) {
  glucose[i] ~ dnorm(solution[i, 1], p[i])
  p[i] <- tau / pow(solution[i, 1], 2)
 solution[1:N, 1:2] <- ivgtt(init[], grid[], theta[],
                                  origin, tol)
                                                      alucose conc.
 init[1] <- G0 + dose / V
                                                            15.0
 init[2] <- 0
 for (i in 1:22) {
  theta[i] <- grid[i]
                                                            10.0
  theta[22 + i] <- insulin[i]
 theta[45] <- Gb; theta[46] <- Ib
                                                             5.0
 theta[47] <- SI
 theta[48] <- SG
 theta[49] <- p2
                                                             0.0
                                                                 0.0
                                                                         50.0
                                                                                  100.0
                                                                                           150.0
                                                                                                    200.0
                                                                                  time
```

# Insulin/glucose/acipimox data

▶ 13 individuals each given IVGTT on 3 occasions (randomized)

- A: overnight fast (control)
- B: 24hr fast + placebo
- C: 24hr fast + acipimox
- Elevate NEFA (non-esterified fatty acid) levels via 24 hour fast – effect on insulin sensitivity and/or secretion?
- Are effects reversed by anti-lipolytic agent acipimox?
- ► Four parameters per IVGTT profile:  $S_1$ ,  $S_G$ , V,  $p_2$  $\rightarrow$  3 × 4 parameters for each individual
- Are there any systematic differences in four basic parameters between 'treatments'?

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#### Statistical model

Let y<sub>ijk</sub> denote kth glucose concentration (taken at time t<sub>ijk</sub>) from individual i on occasion j...

$$y_{ijk} \sim \text{Normal}\left(\mu_{ijk}, \frac{\mu_{ijk}^2}{\tau}\right)$$
$$\mu_{ijk} = \text{IVGTT}(\theta_{ij}, t_{ijk}, I_{ij}(t)), \quad \theta_{ij} = (S_{I_{ij}}, S_{G_{ij}}, V_{ij}, p_{2_{ij}})'$$

• Let 
$$\phi_i = \begin{pmatrix} \theta_{i1} \\ \theta_{i2} \\ \theta_{i3} \end{pmatrix} \dots \quad \mu_{ijk} = \psi(\phi_i, t_{ijk}, l_{ij}(t))$$

 $\phi_i \sim \mathsf{MVN}_{12}(m, \Sigma)$  $m \sim \mathsf{MVN}_{12}(m_0, \mathbf{I}), \quad \Sigma^{-1} \sim \mathsf{Wishart}(12\Sigma_0, 12)$ 

#### Bayes vs. likelihood

- MCMC unhindered by non-linearity can fit desired model:  $\mu_{ijk} = \psi(\phi_i, t_{ijk}, I_{ij}(t))$
- For likelihood based approach have to linearize:

$$\psi \approx \psi(\hat{\phi}_i, t_{ijk}, I_{ij}(t)) + (\phi_i - \hat{\phi}_i) \left. \frac{\partial \psi}{\partial \phi_i} \right|_{\phi_i = \hat{\phi}_i}$$

Disadvantages:

- ► don't know  $\psi \Rightarrow$  don't know  $\frac{\partial \psi}{\partial \phi_i}$  have to evaluate numerically
- no idea how good/adequate approximation is
- difficulties with non-continuous derivatives  $\frac{\partial \psi}{\partial \phi_i}$ , e.g. unknown change-points
- But, much quicker?

#### Bayes vs. likelihood

- Bayesian methods allow incorporation of external evidence:
  - often desirable to incorporate prior knowledge, e.g. from other studies
  - in complex models, may be essential for parameter identifiability
  - may also be essential for reliability of numerical solvers
- Graphical modelling approach allows easy adaptation to complexities of 'real data', e.g.
  - unknown change-points
  - different error distributions
  - measurement error
  - arbitrary hierarchical structures

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BUGS/WBDiff software...

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- Other analyses show decrease in *first phase insulin secretion* also
- These effects partially reversed by acipimox, suggesting lipid-driven mechanisms important
- Decreases in p<sub>2</sub> (takes longer for insulin to work) linked to increases in max overnight growth-hormone levels (independent of changes in NEFA and insulin)

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#### Interstitial-/plasma-glucose data

- Artificial pancreas measures interstitial glucose via current and converts to plasma glucose to determine appropriate insulin input
- ➤ Current can be measured continually via subcutaneous sensor → provides great scope for better management of glucose levels



A. Insulin pump
B. Cannula
C. Glucose sensor
D. Transmitter

#### Interstitial-/plasma-glucose model

 First aim is to characterise relationship between interstitialand plasma-glucose



$$\frac{dIG}{dt} = -p_1IG + p_2PG$$

 Scale/normalize IG so that it is on the same scale as PG: NIG = νIG, where ν = p<sub>1</sub>/p<sub>2</sub>

$$\frac{dNIG}{dt} = -p_1NIG + p_1PG$$

(NIG = PG at steady state)

#### Fits – individuals 2 & 6 / 12



#### Sensor calibration

•  $IG = (C - C_B)/S$  (S = sensitivity,  $C_B = basal \ current$ )

Assume sensor measures current with error

$$C^m = C + \delta = NIG.S/\nu + C_B + \delta$$

Sensor is calibrated every several hours: given current PG value, calculate appropriate scaling factor for mapping C<sup>m</sup> → NIG<sup>m</sup>, i.e. NIG<sup>m</sup> = A.C<sup>m</sup> ⇒

$$NIG^m = F.NIG + B + \eta$$

where  $F = A.S/\nu$ ,  $B = A.C_B$  and  $\eta = A.\delta$ 

#### Sensor calibration continued

- In general there are K calibration times, each giving a different value of A
- If we index time points by j and let P(j) denote the calibration period to which observation j belongs:

$$NIG_j^m = F_{P(j)}NIG_j + B_{P(j)} + \eta_j, \quad \eta_j \sim N\left(0, \sigma_{P(j)}^2\right)$$

where  $NIG_j$  is the solution to  $\frac{dNIG}{dt} = p_1(PG(t) - NIG)$  at time  $t_j$  (with PG(t) as a forcing function)

#### Population model

► Index individuals by *i*:

$$NIG_{ij}^{m} = F_{iP(j)}NIG_{ij} + B_{iP(j)} + \eta_{ij}, \quad \eta_{ij} \sim N\left(0, \sigma_{iP(j)}^{2}\right)$$

Exchangeability assumptions:

$$\begin{split} \log p_{1_i} &\sim \mathsf{N}(\mu_{p1}, \tau_{p1}^{-1}), \quad i = 1, ..., \mathsf{N} \\ \log \sigma_{ik} &\sim \mathsf{N}(\mu_{\sigma}, \tau_{\sigma}^{-1}), \quad k = 1, ..., \mathsf{K} \\ \begin{pmatrix} \log F_{ik} \\ B_{ik} \end{pmatrix} &\sim \mathsf{MVN}_2(\theta_i, \Sigma_{intra}), \quad \theta_i &\sim \mathsf{MVN}_2(\mu_{\theta}, \Sigma_{inter}) \end{split}$$

+ appropriate priors on hyperparameters....

#### Exchangeability assumptions: BUGS code

```
for (i in 1:N) {
 for (k in 1:K) {
   log(sigma[i, k]) <- log.sigma[i, k]
  log.sigma[i, k] ~ dnorm(mu.sigma, tau.sigma)
   F[i, k] <- exp(calib[i, k, 1])
   B[i, k] <- calib[i, k, 2]
  calib[i, k, 1:2] ~ dmnorm(theta[i, ], T.intra[, ])
 theta[i, 1:2] ~ dmnorm(mu.theta[], T.inter[, ])
 loa(p1[i]) <- log.p1[i]
 log.p1[i] ~ dnorm(mu.p1, tau.p1)
}
```

#### Fits – individual 2/12

#### uncalibrated; scaled; scaled + shifted.....



#### Fits – individual 6/12

#### uncalibrated; scaled; scaled + shifted.....



# Estimates for lag-time $\tau = p_1^{-1}$

τ (mins)	Median	25%Q	75%Q
1	17.84	17.09	18.54
2	15.07	14.61	15.53
3	15.88	14.63	17.11
4	10.33	9.38	11.27
5	19.48	19.06	19.94
6	16.06	15.31	16.87
7	16.47	16.03	16.95
8	15.60	14.93	16.35
9	20.53	19.30	21.76
10	11.06	10.42	11.72
11	13.96	13.62	14.25
12	13.78	13.01	14.51
Population	15.23	14.51	15.94

- Accepted value, based on physiology, is around 10 minutes...
- Results show that ~15 minutes more appropriate

#### Explanation

- Additional lag could be due to:
  - time-delay induced by data processing?



#### incorrect model?

- Results backed up by correlating unlagged-NIG<sup>m</sup> with PG at various lags:
  - ho = 0.911 0.932 0.937 0.935

38/42

#### Explanation

- Additional lag could be due to:
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- incorrect model?
- Results backed up by correlating unlagged-NIG<sup>m</sup> with PG at various lags:



#### Extensions/future work

- Long-term goal of current work: simulation of *in silico* population of pseudo-data for fully testing insulin-delivery algorithm (with Roman Hovorka @ Cambridge-Paediatrics and Chen Wei/Michael Lawton @ MRC-BSU)
  - Acknowledge uncertainty in forcing functions
  - Acknowledge uncertainty in calibration times?
  - Modelling autocorrelated residuals
  - Adjust for other biases
  - Extend to modelling of other sensors
  - **۱**...
- Other applied work:
  - Explore use for modelling infectious disease dynamics (with Dani de Angelis, Anne Presanis and Chen Wei @ MRC-BSU
     + Olivier Restif @ Cam-Vet-Med + Christl Donnelly @ Imperial)
  - Use in systems biology (with Lorenz Wernisch @ MRC-BSU)

▶ ....

#### Extensions/future work

#### Methodological

- ► Currently can allow for discrete changes in system, e.g. piecewise constant parameters → extend to continuously changing parameters?
- Facilitate specification of stochastic processes
- Allow for system noise via SDEs
- Allow for lagged/asynchronous systems
- Specification of 'functions' (of dummy variables rather than specific nodes) in BUGS language
- Migration to OpenBUGS
- Þ ..

#### Conclusions

- WBDiff allows specification of (Bayesian) models defined in terms of ODEs
- BUGS/graphical modelling framework provides great scope for dealing with complexities of 'real data', e.g. error distributions, arbitrary model structures, ...
- System currently limited by lack of flexibility re specification of DEs, e.g. forcing functions, lagged systems, ...
- Bayesian approach has several advantages over likelihood-based approach: no approximations, non-continuous derivatives, prior knowledge
- But slower + informative priors may be essential

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- Interstitial-/plasma-glucose data: joint work with Chen Wei (MRC-BSU) and Roman Hovorka<sup>1</sup>
- Experimental host-parasite system: joint work with Olivier Restif (Cambridge Veterinary Medicine)
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